

Video Article

Electron Spin Resonance Micro-imaging of Live Species for Oxygen Mapping

Revital Halevy¹, Lazar Shtirberg¹, Michael Shklyar¹, Aharon Blank¹

¹Schulich Faculty of Chemistry, The Technion, Israel Institute of Technology

Correspondence to: Aharon Blank at ab359@tx.technion.ac.il

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Abstract

This protocol describes an electron spin resonance (ESR) micro-imaging method for three-dimensional mapping of oxygen levels in the immediate environment of live cells with micron-scale resolution¹. Oxygen is one of the most important molecules in the cycle of life. It serves as the terminal electron acceptor of oxidative phosphorylation in the mitochondria and is used in the production of reactive oxygen species. Measurements of oxygen are important for the study of mitochondrial and metabolic functions, signaling pathways, effects of various stimuli, membrane permeability, and disease differentiation. Oxygen consumption is therefore an informative marker of cellular metabolism, which is broadly applicable to various biological systems from mitochondria to cells to whole organisms. Due to its importance, many methods have been developed for the measurements of oxygen in live systems. Current attempts to provide high-resolution oxygen imaging are based mainly on optical fluorescence and phosphorescence methods that fail to provide satisfactory results as they employ probes with high photo-toxicity and low oxygen sensitivity. ESR, which measures the signal from exogenous paramagnetic probes in the sample, is known to provide very accurate measurements of oxygen concentration. In a typical case, ESR measurements map the probe's lineshape broadening and/or relaxation-time shortening that are linked directly to the local oxygen concentration. (Oxygen is paramagnetic; therefore, when colliding with the exogenous paramagnetic probe, it shortens its relaxation times.) Traditionally, these types of experiments are carried out with low resolution, millimeter-scale ESR for small animals imaging. Here we show how ESR imaging can also be carried out in the micron-scale for the examination of small live samples. ESR micro-imaging is a relatively new methodology that enables the acquisition of spatially-resolved ESR signals with a resolution approaching 1 micron at room temperature². The main aim of this protocol-paper is to show how this new method, along with newly developed oxygen-sensitive probes, can be applied to the mapping of oxygen levels in small live samples. A spatial resolution of ~30 x 30 x 100 μm is demonstrated, with near-micromolar oxygen concentration sensitivity and sub-femtomole absolute oxygen sensitivity per voxel. The use of ESR micro-imaging for oxygen mapping near cells complements the currently available techniques based on micro-electrodes or fluorescence/phosphorescence. Furthermore, with the proper paramagnetic probe, it will also be readily applicable for intracellular oxygen micro-imaging, a capability which other methods find very difficult to achieve.

Video Link

The video component of this article can be found at <http://www.jove.com/video/2122/>

Protocol

1. Overview of ESR Micro-imaging

First, we provide a brief explanation of ESR, ESR microscopy, and the various components of our system, and then we will describe the actual imaging experiments.

Electron spin resonance is a spectroscopic technique in which electromagnetic radiation at a specific frequency is absorbed by molecules with unpaired electron spins, placed under an external static magnetic field (Figure 1). ESR is employed in broad areas of science, such as chemistry, biology, physics, and materials science, for the detection and identification of free radicals and paramagnetic centers. It is a powerful method for studying the environment of paramagnetic molecules in live species and provides information about acidity (pH), viscosity, oxygen, and reactive oxygen species concentrations³.

For heterogeneous samples, ESR spectral information can be obtained in a spatially resolved manner (i.e., by obtaining an image), through the use of magnetic field gradients⁴. This is very similar to the more common method of magnetic resonance imaging (MRI) that mainly observes proton spins. Up until now, such ESR imaging techniques were applied for live specimens with relatively large size of a few centimeters and in mm-scale resolution. (For example see Figure 2, taken from reference 5.) A relatively recent development in ESR imaging is the extension of its capabilities from looking at small animals at millimeter-scale resolution to the measurements of millimeter- and sub-millimeter-size samples with micron-scale resolution. This field is known as ESR microscopy, which today can provide 3D ESR images with a resolution approaching 1 micron² (see representative examples in Figure 3).

An ESR microscope is essentially similar to a conventional ESR spectrometer. It has a magnet for generating the static field, a microwave system for spin excitation and signal detection, a probe for holding the sample, and a computerized console to control the acquisition process and data handling. Other components unique to the ESR imaging in general and existing also in ESR microscopy are magnetic field gradient sources, which are part of the electronic system, and gradient coils that are located in the imaging probe. More details about our specific system are shown in the protocol movie and described in reference 2.

2. ESR Micro-imaging Sample Preparation

This stage describes the method for sample preparation for the ESR micro-imaging experiment. At the end of this stage cells are placed on the bottom of a specially-prepared glass ESR microscopy sample container together with a trityl radical⁶ buffer solution. This protocol describes the measurement of cyanobacteria cells and therefore, for other types of cells, proper adjustments may be needed at the sample preparation stage.

1. First, a few squares of absorbent paper with a size of ~400 400 μm are taken and inserted into an Eppendorf tube which is subsequently filled with 1.2 mL of the cyanobacteria suspension (at a concentration of 40 mg/mL).
2. The suspension is centrifuged for 2 minutes at 6000 RPM in a microcentrifuge.
3. Following this, the supernatant buffer is completely removed except for ~50 μL which are left to avoid cyanobacteria dehydration. As a result of this process, the absorbent paper is now saturated by the cyanobacteria cells.
4. Using fine tweezers, a few fibers are extracted from the paper and placed on the bottom of a cup-like specially prepared glass sample holder⁷. Following that a 3 mM of trityl in BG-11 solution^{8,9} (see Scheme 1) is added to the sample holder by the aid of a fine syringe. The holder is then sealed using UV curable glue, leaving a small air outlet open.

Stock 4	Stock 3	Stock 2	Stock 1
H ₃ BO ₃ 2.86g/liter	K ₂ HPO ₄ : 3H ₂ O 4.0g/liter	MgSO ₄ : 7H ₂ O 7.5g/liter	Na ₂ Mg EDTA 0.1g/liter
MnCl ₂ : 4H ₂ O 1.81g/liter			Ferric ammonium citrate 0.6g/liter
ZnSO ₄ : 7H ₂ O 0.222g/liter			Citric acid : 1H ₂ O 0.6g/liter
CuSO ₄ : 5H ₂ O 0.079g/liter			CaCl ₂ : 2H ₂ O 3.6g/liter
COCl ₂ : 6H ₂ O 0.050g/liter			
NaMoO ₄ : 2H ₂ O 0.391g/liter			

Scheme 1. Preparation of BG-11 medium.

3. ESR Micro-imaging Experiments

1. To begin the imaging experiment, turn on the ESR micro-imaging system and insert the sample into the resonator that goes inside the imaging probe.
2. Now, using the computer control software, set the system on "Tune" mode and find the resonance microwave frequency of the probe, which will be used for the ESR measurements.
3. Following that, set the static magnetic field on the value that matches the applied microwave frequency, set the timing parameters for the pulse sequence and observe the ESR signal to make sure that the system functions well and the sample is well-prepared.
4. Then, set the imaging parameters, such as the number of pixels, the strength of the gradients, and the length of the gradient pulses to their required values.
5. Following setup, collect three 3D ESR images by a Hahn echo imaging pulse sequence (Figure 4) with interpulse separation, values of 500, 600, and 700 ns.
6. Light projected at the sample is turned on or off depending on the required experimental conditions.
7. During acquisition, data is automatically saved. These raw data files are then processed via Matlab software script to provide images of the trityl radical concentration and the relaxation time T_2 map, which is translated into an oxygen concentration image via pre-existing calibration.

4. Representative Results

The outcomes of the experiment are several three-dimensional ESR micro-images recorded at different τ values. Typical raw data images are provided in Figure 5. The top three images, measured under dark conditions, are very similar except for reduction in signal intensity. On the other hand, the image pattern changes under light irradiation due to the different relaxation times in different parts of the sample. This data can be processed¹ to obtain an amplitude image, as shown in Figure 6 and also images of the relaxation time, T_2 (Figure 7). The T_2 images are translated into oxygen concentration values via a pre-existing calibration curve that links the oxygen concentration to the relaxation time via the equation:

$$\frac{1}{T_2(C,D)} = \frac{1}{T_2^0(C,D)} + k(C,D)[O_2]$$

Here, T_2^0 is the spin-spin relaxation time of the probe under anoxic conditions (depending on the probe's concentration, C , and its diffusion coefficient, D), and k is a proportionality constant. In most cases, the diffusion coefficient does not vary much for live samples (although, if needed, it can in principle be directly evaluated also by ESR^{6,10}), and the spin concentration is obtained during the imaging process. Therefore, this relation can be used to directly measure oxygen concentration.

Going back to Figure 6, it is evident from the amplitude image that the cyanobacteria cells were located mainly on the right side of the sample holder. Furthermore, based on Figure 7, it is clear that light initiates the production of O_2 and causes a significant increase in the solution's O_2 concentration, mainly in the voxels near the cyanobacteria.

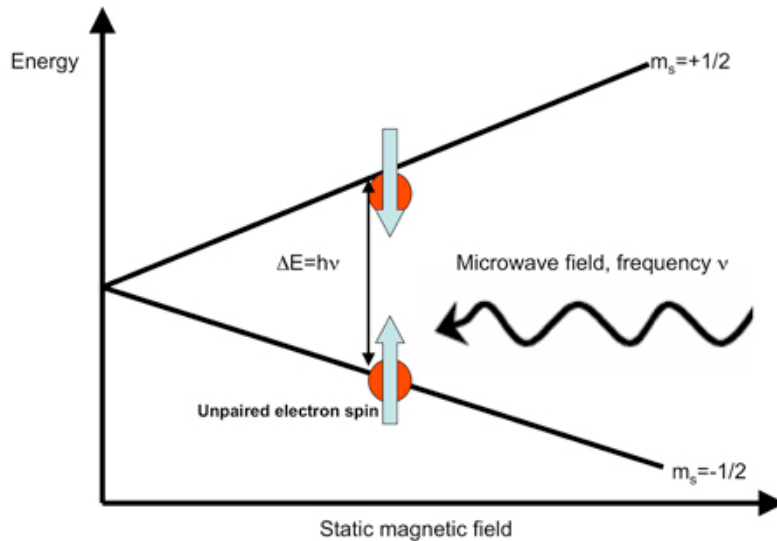
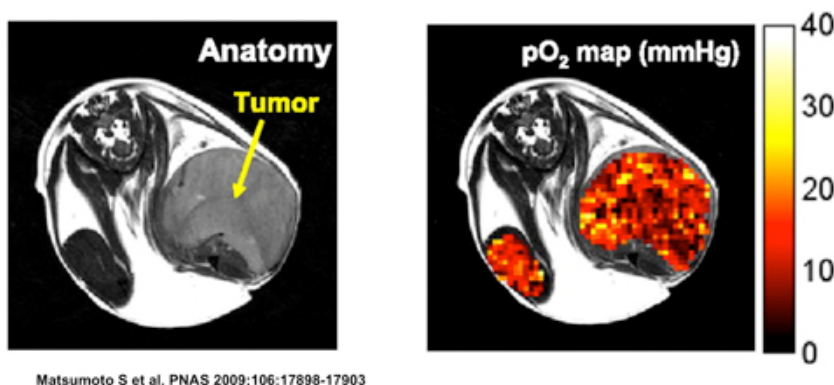


Figure 1: Energy levels in electron spin resonance.



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Figure 2: Typical oxygen concentration image of a Tumor bearing mouse. The image on the left shows the anatomical information, based on an MRI image. A stable free organic radical was injected to the mouse and its ESR characteristics provide the oxygen concentration at its environment (right). ESR-based results are superimposed on MRI anatomical image. Field of view is 32 mm.

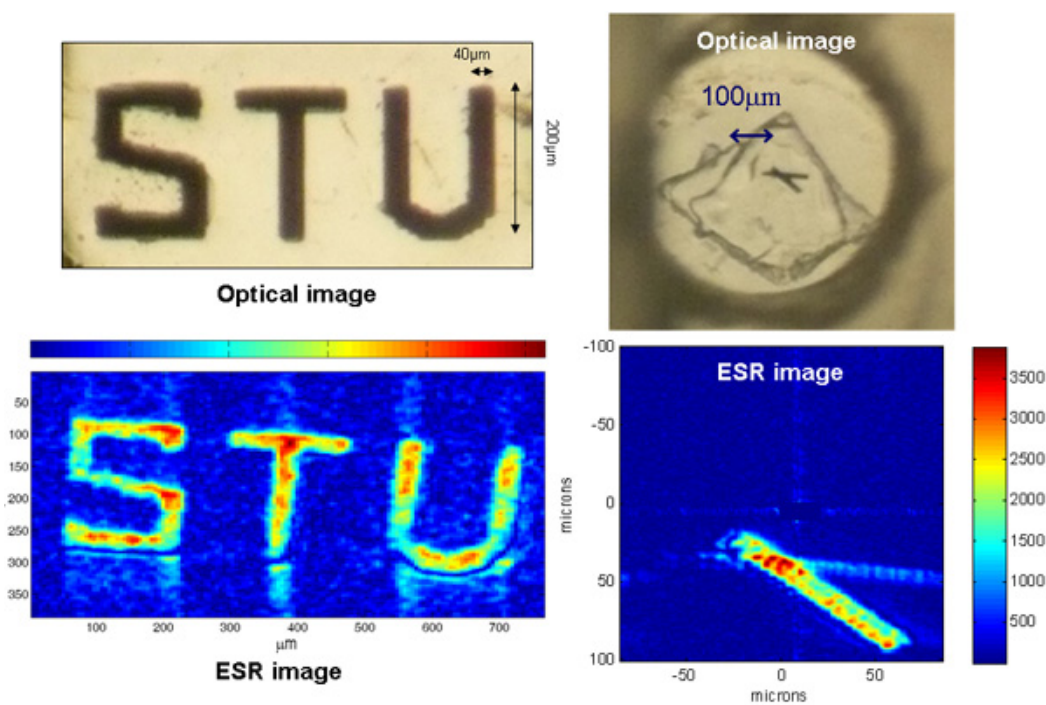


Figure 3: Two examples of high resolution micro-scale ESR images of photolithographically-generated sample with $N@C_{60}$ powder (left) and LiPc paramagnetic crystals (right)

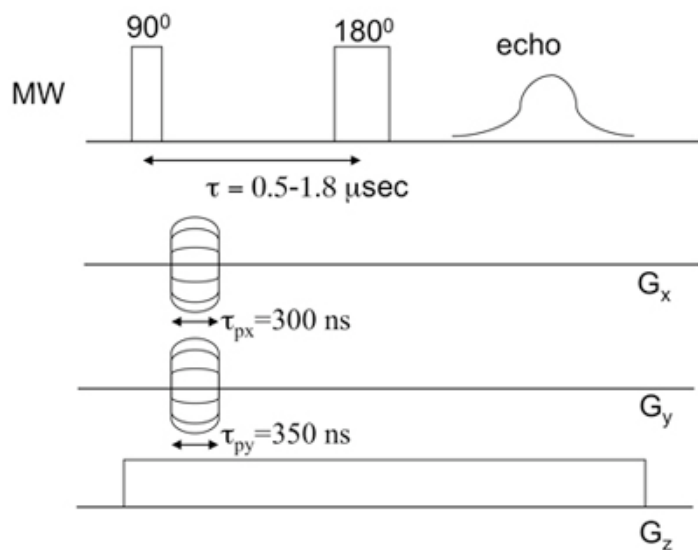


Figure 4: Typical Hahn imaging pulse sequence showing the microwave (MW) and gradient, G_x , G_y and G_z pulses.

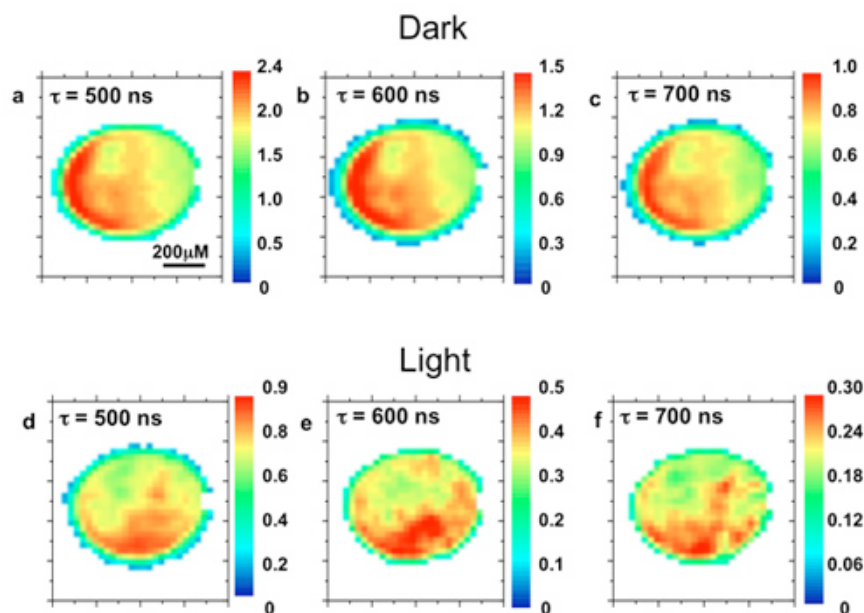


Figure 5: Typical raw-data ESR micro-images: a, b, and c are raw data of the Cyanobacterium sample with no light illumination measured for $\tau = 500, 600, 700$ ns, respectively. Items d, e, and f are the same as a, b, and c but with light illumination. Intensity is plotted in arbitrary scale (but is consistent within each set of three dark or light raw data images)

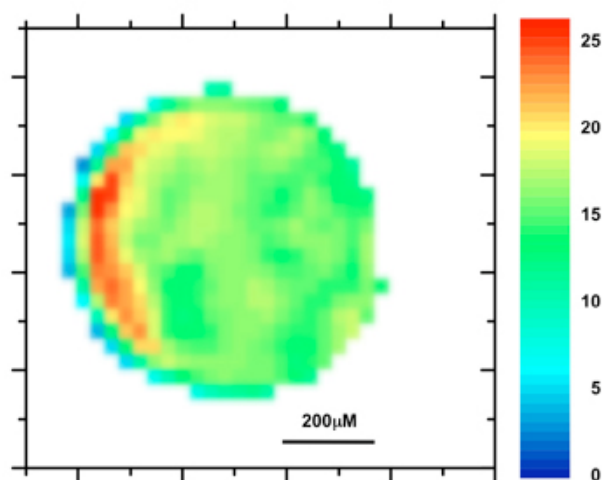


Figure 6: Amplitude image corresponding to the radical concentration in the solution (arbitrary scale).

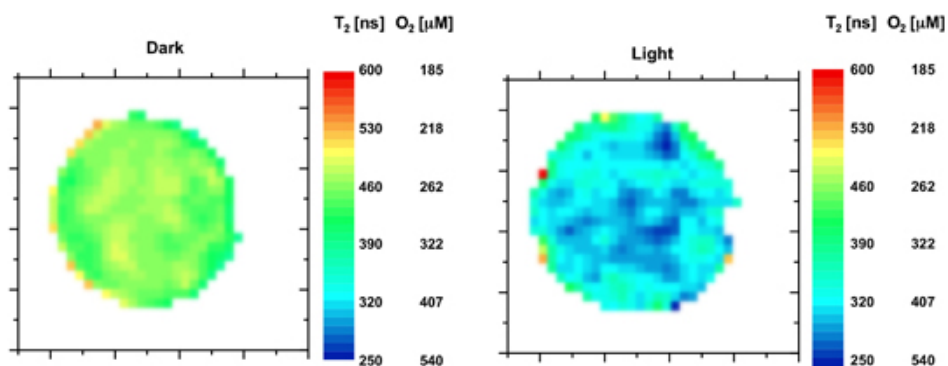


Figure 7: T_2 images and the corresponding $[O_2]$ values under dark (left) and light (right) conditions.

Discussion

This protocol shows how ESR micro-imaging can be applied to map oxygen concentration near live small samples. A spatial resolution of $\sim 30 \times 30 \times 100 \mu\text{m}$ is demonstrated, with near-micromolar oxygen concentration sensitivity and sub-femtomole absolute oxygen sensitivity per voxel. The use of ESR micro-imaging for oxygen mapping near cells complements the currently available techniques based on micro-electrodes or fluorescence/phosphorescence. Furthermore, with the proper paramagnetic probe, it will be readily applicable for intracellular oxygen micro-imaging, a capability which other methods find very difficult to achieve. In the near future we plan on further improving this methodology to provide live sample images with a resolution of a few microns, providing contrast parameters such as super oxide concentration, acidity (pH), probe diffusion coefficient and, of course, oxygen concentration. These capabilities are complementary to the current optical-based methodologies both in terms of contrast type and also of samples characteristics (e.g non-transparent thick samples and, in some cases, intracellular vs. extracellular measurements).

Disclosures

No conflicts of interest declared.

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